Prone versus supine positioning for whole and partial breast radiotherapy: a comparison of non-target tissue dosimetry

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Key words: Breast cancer; Prone breast radiotherapy; Partial breast irradiation; Cardiac dosimetry

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Abstract

**Purpose:** To compare non-target tissue (including left-anterior-descending coronary-artery (LAD)) dosimetry of whole (WBI) and partial-breast irradiation (PBI) planned in prone versus supine positions.

**Methods and materials:** Sixty-five post-lumpectomy breast cancer patients underwent CT-imaging supine and prone. On each dataset, whole-breast clinical-target-volume (CTV) was defined using wire and partial-breast CTV as tumour-bed+15mm. Heart and LAD were outlined in left-breast-affected patients (n=30), and ipsilateral lung and chest-wall in all patients. Tangential-field WBI and PBI plans were generated for each position. Mean LAD, heart, and ipsilateral lung doses (NTD\textsubscript{mean}), maximum LAD (LAD\textsubscript{max}) doses, and chest-wall V\textsubscript{50Gy} were compared.

**Results:** 260 plans were generated. Prone positioning reduced heart and LAD doses in 19/30 WBI cases (mean reduction in LAD-NTD\textsubscript{mean}=7.5Gy) and 7/30 PBI cases (mean reduction in LAD\textsubscript{max}=27.6Gy). However, prone positioning increased cardiac doses in 8/30 WBI (mean increase in LAD-NTD\textsubscript{mean}=8.4Gy) and 19/30 PBI cases (mean increase in LAD\textsubscript{max}=23.7Gy). WB-CTV>1000cm\textsuperscript{3} was associated with improved cardiac dosimetry in the prone position for WBI (p=0.04) and PBI (p=0.02). Prone positioning reduced ipsilateral-lung NTD\textsubscript{mean} in 65/65 WBI and 61/65 PBI cases, and chest-wall V\textsubscript{50Gy} in all WBI cases. PBI reduced normal-tissue doses compared to WBI in all cases, regardless of treatment position.

**Conclusions:** In the context of tangential-field WBI and PBI, prone positioning is likely to benefit left-breast-affected women of cup-size ≥D, and most right-breast-affected women, but to be detrimental in left-breast-affected women of smaller cup size. PBI reliably reduces normal-tissue doses compared to WBI such that eligible women should be encouraged to participate in PBI studies.
Introduction

Whole-breast irradiation (WBI) following breast-conserving surgery (BCS) improves local control and survival from breast cancer but increases non-breast-cancer-related deaths by 1% at 15 years (1). The majority of these deaths are cardiovascular in origin (2) and irradiation of the left-anterior-descending coronary-artery (LAD) is implicated in pathogenesis (3-5). Irradiation of lung, chest-wall and other tissues also contributes to late mortality and morbidity (1, 2). Improvements in radiotherapy techniques have resulted in reduced normal-tissue doses (6), correlating with reduced non-breast-cancer-related mortality (2). Nonetheless doses to the heart, LAD and lung from current standard supine WBI remain significant (7).

Methods by which normal-tissue doses could be decreased include optimization of patient positioning and use of partial-breast irradiation (PBI). Prone positioning for WBI improves dose homogeneity within breast-tissue (8, 9), reduces lung doses (10-12), and reduces wedge requirements with consequent reduction of scattered dose, particularly in women of larger cup-size (10). However, reports comparing cardiac dosimetry from supine versus prone WBI are conflicting. One study using IMRT (13) reported that prone positioning reduced within-field heart volume in 85% of women. However, studies using conventional tangential-field arrangements have failed to show an overall benefit of prone positioning on cardiac dosimetry (11, 14). Furthermore, a study comparing distances between anterior pericardium and chest-wall on supine CT-images and prone MRI (15) found prone positioning to systematically displace supero-lateral aspects of heart-tissue closer to chest-wall, such that prone positioning might be detrimental where target tissues include chest-wall and/or deeply-lying breast tissue. Thus far, LAD doses from prone positioning have not been documented.

PBI could also reduce normal-tissue doses by restricting higher radiation doses to the volume of breast tissue at highest risk of tumour relapse (16). The combination of prone positioning and PBI is particularly attractive in terms of reducing normal-tissue toxicity. A dosimetric comparison of accelerated PBI techniques (14) found that brachytherapy & prone tomotherapy resulted in least
dose to lung and non-target ipsilateral breast tissue (compared with supine 3D-conformal-RT and tomotherapy). However, heart doses again varied between patients, prone tomotherapy benefiting only women with larger breasts and/or lesions further from chest-wall.

Cardiac and, in particular, LAD dosimetry from prone WBI and PBI require further evaluation before prone positioning can be adopted into routine practice. As the majority of centres worldwide continue to use conventional tangential-field arrangements, this study prospectively evaluates non-target tissue exposure from WBI and PBI planned conventionally in supine and prone positions using within-patient comparison. The resulting four-way comparison of prone and supine, WBI and PBI aims to clarify optimal approaches to reducing normal-tissue exposure applicable to the majority of current practices.

**Methods and materials**

This study was approved by the Royal Marsden Committee for Clinical Research and the Regional Ethics Committee. All women had undergone BCS for unifocal T1-2 G1-3 invasive-ductal carcinoma or high-grade ductal-carcinoma-in-situ, at which time titanium-clips were placed in the tumour-bed (TB) according to a UK protocol (17).

**Patient positioning and image acquisition**

Patients underwent non-contrast CT-imaging (slice-thickness 1.5mm, C6 to below diaphragm) in the standard supine position at which time radio-opaque wire was placed at the palpable edge of breast-tissue circumferentially. Patients were repositioned and CT-imaged prone using an in-house-designed platform, with an aperture through which index-breast could fall away from chest-wall [Figure 1]. Radio-opaque wire remained in-situ for prone CT-imaging.

**Target and non-target tissue delineation**

Whole-breast (WB) clinical-target-volume (CTV) was defined using wire plus any additional breast-tissue visualized on CT, limited by 5mm from skin and chest-wall/lung interfaces. Partial-breast CTV was defined as TB (clips plus seroma and/or architectural distortion) expanded by 15mm in 3-
D (limited circumferentially by WB-CTV). Planning-target-volumes (PTV) were generated by addition of 3-D 10mm margins to CTV, limited by 5mm from skin.

Heart and LAD were defined according to published criteria (6). Where LAD was difficult to visualise, its location was inferred from the course of the anterior-interventricular groove (6). Consistent with previous practice, an 10mm axial margin was added to the LAD to allow for delineation-uncertainty, respiratory-motion and cardiac-motion (7). Ipsilateral-lung was outlined using an autocontour tool (edited to exclude major airways). Chest-wall was defined as ipsilateral ribcage and intercostal musculature.

Radiotherapy-planning

For each position, standard opposing tangential-fields were employed such that for WBI, ≥90% of WB-CTV was encompassed by the 95%-isodose and, for PBI, ≥95% of partial-breast CTV was encompassed by the 95%-isodose (according to UK National-Cancer-Research-Institute Intensity-Modulated Partial Organ Radiotherapy (IMPORT) study criteria (18)). Plans fulfilled ICRU dose-homogeneity criteria (19). Dose-distributions were reviewed in 3D and using dose-volume-histogram (DVH) data. 50Gy in 25 fractions over 5 weeks (6-10MV photons) was prescribed to the 100% isodose. MLC leaves were used as required to reduce cardiac doses whilst maintaining satisfactory coverage of WB and PB-CTVs as defined above.

Analysis

NTD$_{\text{mean}}$ (a biologically-weighted mean of dose to normal-tissue normalised to 2Gy fractions (20)) was calculated for heart, LAD, and lung. Maximum-dose to LAD (LAD$_{\text{max}}$) was read from DVH data. The volume of chest-wall receiving 50Gy ($V_{50Gy}$) was calculated.

Differences between heart, LAD and lung-NTD$_{\text{mean}}$, LAD$_{\text{max}}$, and chest-wall $V_{50Gy}$ for supine versus prone WBI, supine versus prone PBI, and supine WBI versus PBI plans were calculated for each patient and compared using the paired t-test or Wilcoxon signed-rank test, as appropriate. Lung and chest-wall doses were compared in all patients. Cardiac doses were compared for left-breast-affected patients only (as a population and by individual patient). Individual-patient cardiac data
were pooled by WB-CTV into tertiles (≤500cm³, 501-1000cm³, >1000cm³) and the likelihood of benefit from prone positioning compared between tertiles using analysis-of-variance.

**Results**

65 women were recruited (30 left-sided: 35 right-sided BC). Mean age was 57 years (range 34-79 years). Self-reported cup-sizes and WB-CTVs are illustrated in figure 2. There was no difference between WB-CTVs delineated in supine and prone positions (p=0.15). Satisfactory coverage of target-volumes was achieved in 100% of plans.

**Cardiac dosimetry**

Heart and LAD doses for the patients with left BC (30 cases, 120 plans) are summarized in table 1 and figure 3. Overall, for the population of left-breast-affected women, there was no significant difference in cardiac parameters between prone and supine positions for either WBI or PBI. Comparing doses within patients, for WBI prone positioning was advantageous in 19/30 patients but disadvantageous in 8/30 patients. The magnitude of the difference between LAD-NTD_{mean} doses was similar whether prone positioning improved or worsened dosimetry [table 2]. In 3/30 patients, prone positioning increased LAD-NTD_{mean} but decreased LAD_{max}. If heart-NTD_{mean} had been the only comparator, 20/30 would have been judged to benefit from prone and 10/30 from supine positioning.

For PBI, prone positioning was advantageous in 7/30 patients, and disadvantageous in 19/30 patients. The magnitude of the difference between LAD_{max} doses was similar whether prone positioning improved or worsened dosimetry. In 4/30 cases, parameters failed to agree on optimal position. If heart NTD_{mean} had been the only comparator, 13/30 patients would have been judged to benefit from prone and 17/30 from supine positioning.

Across all 60 WBI-plans for left-breast-affected cases, LAD_{max} was high (≥29.9Gy) irrespective of treatment position. The mean difference in LAD_{max} for prone versus supine WBI was 4.5±2.5Gy. There was greater inter-patient variability in LAD NTD_{mean} (mean difference in prone versus supine LAD-NTD_{mean}=7.7±2.3Gy³). Conversely, across all 60 PBI plans, LAD-NTD_{mean} was low (mean
LAD-$\text{NTD}_{\text{mean}}$ = 2.8±2.5Gy with a mean difference in prone versus supine LAD-$\text{NTD}_{\text{mean}}$ of 2.6±1.2Gy. There was greater inter-patient variability in LAD$_{\text{max}}$ (mean difference in prone versus supine LAD$_{\text{max}}$ = 25.7±8.5Gy). There was a correlation between heart- and LAD-$\text{NTD}_{\text{mean}}$ ($R= 0.80$ for WBI, $p=0.01$; $R=0.67$ for PBI, $p=0.01$), and between heart-$\text{NTD}_{\text{mean}}$ and LAD$_{\text{max}}$ ($R= 0.44$ for WBI, $p=0.01$; $R=0.59$ for PBI, $p=0.01$).

Analysing results by volumetric-tertile, for WBI there was a significant benefit of prone positioning on cardiac doses for women with breast volumes >1000cm³ ($p=0.04$) [figure 4]. All women of D-cup or above benefited from the prone position with the exception of one patient (G cup) whose TB was in the axillary-tail. In the context of PBI, there was a significant benefit of prone positioning on LAD$_{\text{max}}$ doses ($p=0.02$) but not on heart- ($p=0.09$) or LAD-$\text{NTD}_{\text{mean}}$ ($p=0.14$) doses for women with breast-volumes >1000cm³. A breast volume of ≤1000cm³ was significantly associated with a benefit from supine positioning in the context of both WBI and PBI.

Figure 5 demonstrates that in both small- and large-breasted women, heart-tissue moves anteriorly in relation to chest-wall. However, the larger breast is pulled further anteriorly than the smaller breast owing to the greater weight of breast-tissue such that shallower tangents can be placed thereby sparing a greater volume of normal-tissue.

Cardiac doses were significantly lower for PBI as compared to WBI ($p<0.001$). Mean reductions in heart-$\text{NTD}_{\text{mean}}$ were $0.7±0.1\text{Gy}_3$ (supine) and $0.5±0.1\text{Gy}_3$ (prone). Mean reductions in LAD-$\text{NTD}_{\text{mean}}$ were $9.4±0.2\text{Gy}_3$ (supine) and $6.1±1.5\text{Gy}_3$ (prone). Mean reductions in LAD$_{\text{max}}$ were $22.7±6.2\text{Gy}$ (supine) and $11.9±5.4\text{Gy}$ (prone).

**Lung and chest-wall dosimetry**

Ipsilateral-lung $\text{NTD}_{\text{mean}}$ doses (65 cases, 260 plans) are summarised in table 1 and figure 3d. Prone, as compared to supine, positioning significantly reduced ipsilateral-lung $\text{NTD}_{\text{mean}}$ in 65/65 WBI cases (mean reduction=3.5±0.5Gy$_3$ ($p<0.001$)), and 61/65 PBI cases (mean reduction=1.1±0.2Gy$_3$($p<0.001$). In 4/65 PBI cases, ipsilateral-lung-$\text{NTD}_{\text{mean}}$ was similar in both positions because TBs were located at the lateral edge of breast-tissue such that PB-CTV coverage would
have been compromised by shallower tangents in the prone position. Ipsilateral-lung NTD_{mean} was significantly lower for PBI as compared to WBI (mean reduction = 2.9±0.3Gy supine) and 0.4±0.1Gy prone (p<0.001)).

Prone positioning significantly reduced chest-wall V_{50Gy} for WBI only (table 1, figure 3e). Use of supine PBI, compared to WBI, reduced chest-wall V_{50Gy} by 17±7cm^3 (p<0.001). There was no difference between chest-wall V_{50Gy} for prone PBI versus WBI (p=0.08).

**Discussion**

This study aimed to compare normal-tissue (including left-anterior-descending coronary-artery (LAD)) dosimetry from conventional tangential-field whole- and partial-breast radiotherapy planned in prone versus supine positions.

*Cardiac dosimetry*

We found the effects of prone positioning upon both heart and LAD doses to be variable between patients, consistent with previous studies (10, 14). Around two-thirds of patients planned for WBI benefited from prone positioning, with mean improvements in heart-NTD_{mean}, LAD-NTD_{mean}, and LAD_{max} of 0.4Gy, 7.0Gy and 4.9Gy respectively. However, in a third of patients, prone positioning would have increased cardiac doses to a similar extent (table 2). Only a quarter of patients planned for PBI would have benefited from prone positioning, with mean improvements in heart-NTD_{mean}, LAD-NTD_{mean} and LAD_{max} of 0.2Gy, 2.1Gy, and 27.6Gy respectively. In two-thirds of PBI cases, prone positioning would have increased cardiac doses to a similar extent (table 2).

We found a significant benefit of prone positioning upon heart/LAD doses for women of WB-CTV>1000cm^3 (equivalent to UK cup size ≥D) for both WBI and PBI, consistent with previous work reporting a trend towards a significant benefit of prone positioning upon heart dose in women of breast cup-size ≥E (11). Our findings are also consistent with work reporting that heart-tissue moves towards chest-wall in patients positioned prone (15). Only patients in whom breast-tissue falls anteriorly in relation to chest-wall in the prone position (such that shallower tangents can be
placed) are likely to gain from prone treatment. Otherwise, where smaller breasts are not pulled anteriorly, tangents are likely to encompass more cardiac tissue in the prone position.

Not all patients of large breast size in our study had better cardiac dosimetry in the prone position. One patient (cup size G) had a tumour-bed in the axillary tail which could not be encompassed by WBI-tangents without increasing their depth and therefore normal-tissue doses. There may be other predictive factors including heart-size, chest-wall breadth and curvature that our study is underpowered to detect.

The proportion of women benefitting from prone positioning in our study differed from interim reports of the largest ongoing comparative study of prone versus supine WBI, which suggest that prone positioning reduces in-field heart volume in the majority (85%) of left-sided BC patients (n=200)(13). Discrepancies between results could be due to use of volumetric rather than dosimetric comparators and/or to use of IMRT rather than conventional tangential-fields. Using IMRT, an in-field heart volume of 0cm$^3$ is likely to be achievable in a proportion of patients in both supine and prone positions. In this case, the effect of prone positioning upon heart is assumed to be neutral but the prone position might still be judged “optimal” based on reduced in-field lung volume compared to the supine position. This approach does not however detect differences in lower-dose irradiation of cardiac tissues thereby overestimating the clinical benefits of prone positioning in comparison to our study. Our additional use of LAD-dosimetry to discern optimal treatment position might also have lead to differing results. Although heart- and LAD-NTD$_{mean}$ correlated reasonably well, there was disagreement between heart and LAD doses over optimal treatment position in 7/60 plans. Had heart NTD$_{mean}$ been the only comparator, 20/30 and 13/30 patients would have benefited from prone treatment in the context of WBI and PBI respectively. Another source of discrepancies could be the method by which WB-CTV is defined. Clinicians’ decisions on where to place the posterior RT-field border in order to achieve target-volume coverage will significantly impact upon doses to tissues close to chest-wall. Our study used a method of WB-CTV definition agreed to be more representative of the true volume than standard
anatomical landmarks (21). Wire-delineated breast tissue shifts anteriorly in the prone position but is consistently included as WB-CTV. Our WB-CTVs were comparable between positions with no significant difference in percentage volume covered. Additionally, all of our cases had titanium-clip-defined TB volumes, without which, coverage of PB-CTV at depth cannot be ensured (22).

The clinical impact of differences in cardiac doses of the magnitude described above is difficult to quantify as radiation parameters determining excess cardiovascular disease (CVD) risk are poorly understood. Gagliardi (23) used the relative-seriality model to quantitatively describe the dose-response relationship for excess cardiac mortality and found a low dependence of this endpoint upon irradiated-heart-volume, concluding that cardiac mortality is more likely to be reduced by decreasing dose than by restricting irradiated volume. Borger et al (24) also found no relationship between maximum heart distance (MHD) (a correlate of irradiated-heart-volume) and risk of CVD but reported that, even where MHD=0mm, more cardiotoxic effects occurred following left-sided as compared to right-sided-RT suggesting that differences in doses <25Gy may be important. Other data supporting the hypothesis that low-dose radiation increases CVD risk come from atomic-bomb survivors (4Gy single exposure) (25), patients treated with RT for peptic-ulcer disease (mean heart dose 1.6-3.9Gy) (26), patients treated with para-aortic irradiation for testicular cancer (~1Gy scattered heart dose) (27) and radiation workers (28). Cardiac variables which encompass volumes of cardiac tissue irradiated to low doses such as heart-NTD mean have shown a strong correlation with mortality (29). Optimal positioning in our study decreased mean heart-NTD mean from ~1.2 to ~0.8Gy3 for WBI, and from ~0.5 to ~0.3Gy3 for PBI. Based on the evidence above, the risks of low-dose cardiac irradiation are not negligible. However, the dose-effect relationship at these dose-levels is difficult to define and the clinical consequences of such small differences unquantifiable.

Meanwhile, other studies suggest that LAD dose is the most relevant exposure variable (3-5). Retrospective review of patients irradiated between 1977-95 found a significantly higher prevalence of cardiac stress-test abnormalities amongst left- versus right-side-irradiated patients,
70% of which were in LAD territory. Others correlate a fall in mean LAD doses from breast RT over the past 30 years with a decrease in CVD over the same period. Furthermore, it may be that Gagliardi’s finding of a low dependence of cardiac mortality upon irradiated-heart-volume relates to the fact that the LAD is likely to remain within the high-dose volume from a tangential-field arrangement even at low irradiated-heart-volumes. Optimal positioning in our study decreased mean LAD-NTD from ~14 Gy to 6 Gy for WBI, and from ~4 Gy to 1.5 Gy for PBI. Reductions in dose of these magnitudes could be associated with a significant reduction in CVD. As atherosclerosis anywhere along the LAD could cause CVD, LADmax is a relevant additional variable. Optimal positioning in our study decreased mean LADmax from ~49 Gy to 45 Gy for WBI, and from 42 Gy to 15 Gy for PBI. The latter could be particularly significant depending partly upon the threshold dose for atherosclerosis, Gagliardi’s work suggesting that the risk of cardiac mortality rises steeply above doses of around 20 Gy regardless of the volume irradiated. Whether dosimetric differences of these magnitudes continue to be relevant in the context of 5 mm set-up errors and physiological changes in heart and intra-thoracic volume with respiration (each of which may cause interfraction variations in normal-tissue doses) remains to be determined.

**Lung and chest-wall dosimetry**

Our study confirms previous reports that prone positioning reduces mean lung doses for both WBI and PBI and furthermore demonstrates that benefits are applicable to women of all cup-sizes. The main threat of death in relation to irradiation of lung-tissue is from low-dose stochastic effects rather than from high-dose deterministic effects, the relative-risk of death from second-primary lung cancer ranging from 1.5 to 2.8 at 15 years, with odds ratios of up to 37.6 reported in smokers. Data on lung-cancer deaths in ~9000 women irradiated in 1935-1971 (30) suggest a dose-response relationship with an incremental RR of 0.2 per Gy to ipsilateral-lung (equating to 9 cases of RT-induced lung cancer/ year/10,000 women receiving a lung dose of 10 Gy and living to 10 years). The SEER registry cohort demonstrates a similar relationship.
between mean lung dose and risk of second-primary lung-cancer (2) in women irradiated in 1973-2001. Our mean lung-NTD\textsubscript{mean} for supine WBI was 3.7Gy. Prone positioning reduced this to 0.3Gy. Based on evidence above, this reduction in dose might prevent around 3 lung cancers/year/10000 women living to 10 years post-RT. The effect may be larger however in women who smoke, in whom prone treatment might be particularly beneficial.

The START trial suggests that 40% of women experience chest-wall discomfort at 10 years post-RT (33), whilst the incidence of rib-fracture following WBI is reported to be 0.3-2.2% (34, 35). A recent study of external-beam-accelerated-PBI found the incidence of chest-wall pain and rib fracture to relate to the volume of chest-wall receiving 35Gy or more (based on 38.5Gy/10 fractions 5 days (36)). This is equivalent to around 48Gy in 2Gy fractions and is in keeping with tolerance doses published by Emami (37) (TD\textsubscript{5/5} ribcage ~50Gy). Therefore chest-wall V\textsubscript{50Gy} could be considered a reasonable parameter by which to compare radiotherapeutic approaches in terms of late chest-wall discomfort. Prone positioning significantly reduces chest-wall V\textsubscript{50Gy} in WBI and therefore warrants consideration as a technique by which chest-wall morbidity might be reduced.

The future of prone breast RT

In departments where conventional tangential-field WBI is standard, prone positioning is likely to benefit most left-breast-affected women of cup size ≥D, and nearly all right-breast-affected women. A current priority is to establish whether or not the position is reproducible in order that dosimetric benefits can be realized. In the context of tangential-field PBI, prone positioning benefited fewer left-breast-affected women but still reduced the LAD\textsubscript{max} by over 20Gy in many large-breasted women. Further work in this setting might be helpful in establishing predictive factors for deciding optimal treatment position in left-breast-affected women. For right-breast-affected women, reductions in lung and chest wall doses are small and a change of treatment technique may not therefore be warranted. Based on our results, prone positioning for either WBI or PBI is not recommended in left-breast-affected women of cup-size<C as cardiac doses may be significantly increased in comparison to supine treatment.
**PBI versus WBI**

The normal-tissue dosimetric advantages of PBI have been assumed but not proven. Indeed a recent study reported that 3D-conformal PBI increased the volume of lung exposed to low-dose radiation whilst decreasing the volume of tissue exposed to higher-dose radiation (38). We found that supine PBI reduced mean heart-NTD$_{\text{mean}}$ (by 0.6Gy), mean LAD-NTD$_{\text{mean}}$ (9Gy), mean LAD$_{\text{max}}$ (23Gy), mean ipsilateral-lung-NTD$_{\text{mean}}$ (3Gy) and mean chest-wall $V_{50\text{Gy}}$ (17cm$^3$) compared to supine WBI. With dose-sparing of this magnitude, it seems likely that PBI will reduce long-term cardiovascular side-effects of breast RT, reduce second-primary lung malignancies by around 2 lung cancers/year/10000 women at 10 years post-RT, and reduce the incidence of late chest-wall discomfort. PBI should be considered the optimal strategy for reducing late morbidity of breast RT but is currently only available in trials for which many women are ineligible. Prone positioning still has a role in reducing normal-tissue toxicity in women requiring adjuvant WBI.

**Conclusions**

In the context of tangential-field WBI and PBI, prone positioning is likely to benefit left-breast-affected women of cup-size $\geq$D, and most right-breast-affected women, but to be detrimental in left-breast-affected women of smaller cup size. PBI reliably reduces normal-tissue doses compared to WBI such that eligible women should be encouraged to participate in PBI studies.
References


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nested case-control study regarding absorbed dose to the heart and 11 anatomical substructures of the heart. *Radiother Oncol* 2008;xx:xx.


Table 1. Mean normal tissue doses (with 95% confidence intervals)

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<tr>
<th></th>
<th>Supine WBI</th>
<th>Prone WBI</th>
<th>Difference between prone &amp; supine WBI</th>
<th>p</th>
<th>Supine PBI</th>
<th>Prone PBI</th>
<th>Difference between prone &amp; supine PBI</th>
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<tr>
<td>Heart-NTD_mean (Gy_3)</td>
<td>1.0±0.1</td>
<td>0.9±0.1</td>
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<td>0.14</td>
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<td>Ipsilateral-lung NTD_mean (Gy_3)</td>
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<tr>
<td>Chest-wall V_{50Gy} (cm(^3))</td>
<td>20±7</td>
<td>2±1</td>
<td>18±7</td>
<td>&lt;0.001</td>
<td>3±2</td>
<td>1±1</td>
<td>2±2</td>
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Table 2: Comparison of cardiac doses according to superiority of patient position for WBI and PBI

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<td>N=19</td>
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<tr>
<td>WBI</td>
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<td></td>
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<tr>
<td>Heart-NTD$_{\text{mean}}$ (Gy$_3$)</td>
<td>Supine 0.7±0.1, Prone 1.1±0.3, Difference 0.5±0.2, p 0.01</td>
<td>Supine 1.2±0.2, Prone 0.8±0.1, Difference 0.4±0.1, p &lt;0.001</td>
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<td>LAD-NTD$_{\text{mean}}$ (Gy$_3$)</td>
<td>Supine 5.1±2.2, Prone 13.5±3.2, Difference 8.4±2.5, p &lt;0.001</td>
<td>Supine 14.6±2.4, Prone 7.5±2.1, Difference 7.0±2.1, p &lt;0.001</td>
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<td>LAD$_{\text{max}}$ (Gy)</td>
<td>Supine 45.1±4.7, Prone 49.1±1.8, Difference 3.9±3.3, p 0.05</td>
<td>Supine 49.7±0.4, Prone 44.9±1.9, Difference 4.9±1.7, p &lt;0.001</td>
</tr>
<tr>
<td>PBI</td>
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<td></td>
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<tr>
<td>Heart NTD$_{\text{mean}}$ (Gy$_3$)</td>
<td>Supine 0.3±0.1, Prone 0.5±0.1, Difference 0.2±0.1, p 0.002</td>
<td>Supine 0.4±0.1, Prone 0.3±0.1, Difference 0.2±0.1, p 0.10</td>
</tr>
<tr>
<td>LAD NTD$_{\text{mean}}$ (Gy$_3$)</td>
<td>Supine 1.7±0.7, Prone 4.6±1.4, Difference 3.0±1.1, p &lt;0.001</td>
<td>Supine 3.4±1.4, Prone 1.3±0.8, Difference 2.1±1.4, p 0.03</td>
</tr>
<tr>
<td>LAD$_{\text{max}}$ (Gy)</td>
<td>Supine 19.0±7.6, Prone 42.7±3.6, Difference 23.7±6.5, p &lt;0.001</td>
<td>Supine 41.9±5.4, Prone 14.3±12.7, Difference 27.6±10.5, p 0.003</td>
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Figure Captions

Figure 1. Prone platform including polycarbonate centrepiece with aperture, polystyrene head and body supports, and polystyrene wedge to support contralateral breast

Figure 2. Distributions of patients by a) cup size and b) whole-breast clinical-target volume

Figure 3a-e. Box and whiskers plots displaying normal tissue dosimetry a) Heart-NTD<sub>mean</sub> b) LAD-NTD<sub>mean</sub> c) LAD<sub>max</sub> (figures 3a-c include left-breast-affected women only, n=30) d) Ipsilateral-lung NTD<sub>mean</sub> (n=65) e) Chest-wall V<sub>50Gy</sub> (n=65). Black dots= outliers (numbers represent trial-numbers)

Figure 4. Relationship of breast-tissue (cyan-outline), heart (pink-outline), and left-anterior-descending coronary-artery (red-outline with cyan-bullseye) to chest-wall for: i) woman of cup-size B and ii) woman of cup-size F a) supine and b) prone

Figure 5. Mean difference in cardiac variables (supine minus prone) expressed by whole-breast clinical-target volume tertile for a) WBI and b) PBI. (Negative values= benefit of prone position)
Figure 1.
Figure 2.

a) Self-reported cup size (UK) vs. Number of patients

b) Whole breast clinical target volume vs. Number of patients
Figure 3.

(a) Heart NTD$_{\text{mean}}$ (Gy$^3$) comparison between supine and prone WBI/PBI.

(b) LAD NTD$_{\text{mean}}$ (Gy$^3$) comparison between supine and prone WBI/PBI.
Figure 4.

(a) Supine minus prone values for different WB CTV volumes, showing mean heart NTD (Gy3) and mean LAD NTD (Gy3) for different volume ranges.

(b) Supine minus prone values for different WB CTV volumes, showing mean heart NTD (Gy3) and mean LAD max dose (Gy) for different volume ranges.